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recordings and LORETA-computed intracortical activity showed, in the alpha1 frequency band, better cognitive performance with increased cortical activity in the left insula. **Conclusion** The results point to a 'normalization' of the EEG power spectrum due to medication, and the intracortical localization of these effects showed an increase of cortical activity in frontal, parietal, and temporal regions that are well-known to be affected in Alzheimer's disease. The topographic convergence of the present results with the memory network proposed by Vincent et al. (J. Neurophysiol. 96:3517–3531, 2006) leads to the speculation that in our group of patients, rivastigmine specifically activates brain regions that are involved in memory functions, notably a key symptom in this degenerative disease.

Keywords Alzheimer's disease · Rivastigmine · Cholinesterase inhibitors · EEG · Spectral analysis · Source localization · LORETA functional imaging

Introduction

Alzheimer's disease (AD) is a degenerative process, characterized by the loss of cholinergic neurons in the basal forebrain nuclei (Whitehouse et al. 1981). This degeneration of cortical projection of cholinergic neurons results in a deficiency of acetylcholine in the neocortex and hippocampus (Geula 1998), and the deficit is, to some extent, responsible for the underlying cognitive and neuropsychiatric dysfunction.

Based on the cholinergic hypothesis, cholinesterase inhibitors (ChE-I) currently is the most frequently recommended symptomatic treatment (Doody et al. 2001). Clinical studies have confirmed the efficacy of ChE-I treatment in AD on cognitive and neuropsychiatric symptoms

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(see Bullock and Dengiz 2005, for a review) and a series of recent positron emission tomography (PET) and single photon emission computed tomography (SPECT) studies reported an increase of cortical activity due to ChE-I therapy at temporo-parietal and frontal regions (e.g., Bohnen et al. 2005; Ceravolo et al. 2004; Mega et al. 2001), in the hippocampus (Mega et al. 2001), and in the posterior cingulum (Bohnen et al. 2005; Ceravolo et al. 2004), i.e., in regions that have been shown to be the most affected cortical areas in AD (e.g., Jagust et al. 1997).

Because electroencephalography (EEG), as a noninvasive method, can be applied repeatedly, it is a suitable tool to assess the course of the cortical activity during psychoactive medication. The spontaneous EEG, i.e., the recording of the brain electrical activity during resting, is a standard procedure. It is well established that patients with clinically diagnosed AD show a slowing of their EEG frequency during resting compared with healthy age-matched subjects: AD patients have increased power in slow frequency EEG activity (delta and theta frequency bands) and decreased power in fast frequency EEG activity (alpha and beta frequency bands; e.g., Gianotti et al. 2007; Schreiter-Gasser et al. 1993). Moreover, EEG has also been shown to reflect the progressive cortical dysfunctioning correlated with the cognitive impairment in AD patients (e.g., Gianotti et al. 2007; Schreiter-Gasser et al. 1994).

Relationships between cholinergic system and EEG power spectrum, especially in slow EEG frequencies, have been recognized in a variety of animal (e.g., Crouzier et al. 2006; Keita et al. 2000) and human studies (e.g., Riekkinen et al. 1991; Hartikainen et al. 1992). Treatment with ChE-I has been shown to decrease the amount of slow EEG activity, i.e., to ‘normalize’ the EEG power spectrum (e.g., Adler and Brassen 2001; Balkan et al. 2003; Jelic et al. 1998; Kogan et al. 2001).

Unfortunately, single or multichannel EEG has the limitation that the signals that are measured on the head surface do not directly indicate the location of the active neuronal generators in the brain. To solve this so-called ‘inverse problem’, the three-dimensional source localization method, low resolution electromagnetic tomography (LORETA, Pascual-Marqui et al. 1994, 1999), was used.

Using this method, Babiloni and colleagues showed correlations in the EEG delta and alpha frequency bands between the strength of the intracerebral sources and the severity of global cognitive decline (Babiloni et al. 2006a), and the severity of focused attention decline (Babiloni et al. 2007). Of particular interest for the present investigation is the only previous LORETA ChE-I treatment study done by Babiloni et al. (2006b): Globally, they did not show any significant shift towards normalization in the cortical activity after 1 year of donepezil treatment, but dividing

their AD subjects into two groups based on their cognitive performance differences (‘responders’ vs. ‘nonresponders’), the authors found that ‘responders’ showed a lesser reduction of occipital and temporal alpha1 activity compared to nonresponders, thus pointing to a correlation between the difference of cognitive performances and the difference of alpha1 cortical activity after 1 year of donepezil treatment.

All these LORETA studies used a macroregion rather than a voxel-wise approach, thus reducing the number of statistical tests but forgoing a higher spatial resolution.

Using a voxel-wise approach, a previous LORETA functional imaging study on a group of non-medicated mild to moderate AD patients specified that increases in slow frequency EEG activity (delta and theta frequency bands) and decreases in fast frequency EEG activity (alpha2, beta1, beta2, and beta3 frequency bands) affected different cortical areas while largely sparing prefrontal cortex (Gianotti et al. 2007); the study also showed that decreased delta activity at left parietal areas and increased alpha1 activity at left temporal areas correlated with better cognitive performance measured with the Mini Mental State Examination (MMSE, Folstein et al. 1975).

In the present study, multichannel EEG was recorded in a group of 16 AD patients at baseline and after 3 months of rivastigmine treatment to monitor the electrocortical effects of ChE-I using LORETA functional imaging. A group of 16 matched controls was also recorded to confirm the typical reported aberrations of AD resting EEG (see above).

Based on the studies reviewed above, we hypothesized that our patients under rivastigmine will show a ‘normalization’ of their power spectrum on the scalp, particularly a decrease of slow frequency activity and an increase of cortical activity at temporo-parietal, frontal, cingulate, and hippocampal regions. Furthermore, we hypothesized that the expected cognitive amelioration under rivastigmine will positively correlate with an increase of cortical activity localized in left-lateralized temporo-parietal areas as predicted by our earlier LORETA study reviewed above.

Materials and methods

Subjects

Sixteen patients with clinically diagnosed AD (mean age: 77.4 years, S.D.: 6.2; eight men and eight women; handedness: 5 right, 11 unknown) admitted to the Department of Geriatric Psychiatry at the University Hospital of Zurich, Switzerland, took part in the study. All patients met the diagnosis of probable or possible AD according to the NINCDS-ADRDA (McKahn et al. 1984) criteria and the ICD-10 Classification of Mental and Behavioral Disorders

(WHO 1993). Patients with possible vascular dementia, mixed AD-vascular dementia, and major depression were ruled out by neuropsychological testing, laboratory investigations, and brain structural imaging (computed tomography or magnetic resonance tomography). All patients were enrolled for the participation in an open-label treatment study with rivastigmine. The first, baseline EEG was recorded before rivastigmine therapy (session t_0). The second, follow-up EEG recording was done 3 months after treatment initiation (session t_1). In all patients, other centrally active medication was terminated 1 week before the EEG recordings. MMSE was administered at the beginning of both recording sessions to assess the severity of the disease and to monitor cognitive changes due to the medication. A group of 16 age- and gender-matched healthy volunteers was used as controls (mean age=74.0 years, S.D=8.5). Cognitive impairment was excluded by clinical interviews and neuropsychological testing. The study was approved by the Ethics Committee of the University Hospital Zurich. Written informed consent was obtained from all subjects.

EEG recordings

Vigilance-controlled multichannel EEG was recorded using a Nihon-Kohden “NeuroFile” system (electrode impedance <5 kOhm, 1–120 Hz bandpass, 256 samples/s). Nineteen electrodes covering the entire scalp were placed according to the International 10-20 System (Nuwer et al. 1998) at the following locations: Fp1/2, F7/8, F3/4, FZ, T3/4, C3/4, CZ, T5/6, P3/4, Pz, O1/2. The average of F3 and F4 was used as recording reference. Electrodes at the left outer canthus and above and below the left eye were used to monitor vertical and horizontal eye movements. Subjects were seated in a sound- and electrically shielded chamber with dim illumination. They were instructed that the experiment involved EEG recording during resting with open or closed eyes. The instructions about eye opening/closing were given via intercom. The following protocol was used for every subject: (1) 20 s eyes open, 20 s eyes closed; (2) 20 s eyes open, 80 s eyes closed; (3) 20 s eyes open, 80 s eyes closed; (4) 20 s eyes open, 20 s eyes closed. Only data from the total of 200 s eyes closed conditions were analyzed.

For each subject, the EEG recordings were carefully inspected off-line on a PC display for artifacts caused by eye and head movements, muscle activity, sweating, and technical problems. Using a moving, nonoverlapping window, all artifact-free 2-s epochs were selected for further analyses. On the average across patients and sessions, there were 20.3 (SD=1.5) 2-s epochs available, and across controls there were 19.7 (SD=2.0), with no significant difference between the two sessions and between groups.

EEG data analysis

Spectral analysis

The EEG data were recomputed against the average reference (Lehmann and Skrandies 1980). Fast Fourier Transformation (FFT using a square window) was applied to each epoch and channel to compute the spectral power density with 0.5-Hz frequency resolution. For each subject and for each session, the spectra for each channel were averaged over all epochs.

For descriptive statistics, mean power values over subjects were computed for each session.

Absolute spectral power values for each subject, session, and channel were integrated for the following seven independent frequency bands (Kubicki et al. 1979): delta (1.5–6 Hz), theta (6.5–8 Hz), alpha1 (8.5–10 Hz), alpha2 (10.5–12 Hz), beta1 (12.5–18 Hz), beta2 (18.5–21 Hz), and beta3 (21.5–30 Hz). Before statistical analysis, log transformation was applied to normalize the distribution of absolute power values (Gasser et al. 1982).

A two-way analysis of variance (ANOVA) with *groups* (2 levels: AD patients and controls at time t_0) as between-subject factor and *electrode location* (19 levels: Fp1/2, F7/8, F3/4, FZ, T3/4, C3/4, CZ, T5/6, P3/4, Pz, O1/2) as within-subject factor was carried out for each frequency band separately.

Subsequently, only for the AD group, a two-way ANOVA with *session* (two levels: t_0 and t_1) and *electrode location* (19 levels: Fp1/2, F7/8, F3/4, FZ, T3/4, C3/4, CZ, T5/6, P3/4, Pz, O1/2) as within-subject factors was carried out for each frequency band separately. Paired *t* tests were used as post hoc tests. Throughout, two-tailed *p* values are reported.

The MMSE data were normally distributed according to the Shapiro–Wilk test. Correlations between differences in power density in the seven frequency bands (session t_1 –session t_0) and differences in the clinical severity measured with the MMSE (session t_1 –session t_0) were computed using Pearsons’ product-moment correlations.

LORETA functional images of electric neuronal activity

From scalp-recorded electric potentials, LORETA (Pascual-Marqui et al. 1994, 1999) estimates the distribution of electric source activity by assuming similar activation among neighboring neuronal ensembles, an assumption implemented by computing the “smoothest” of all possible activity distributions.

This three-dimensional source localization technique has recently received important cross-modal validation from studies combining LORETA with functional magnetic

resonance imaging (MRI; Mulert et al. 2004), structural MRI (Worrell et al. 2000), and PET (Oakes et al. 2004). Especially concerning AD, it has been shown that the spatial pattern of glucose metabolism correlates with the localization of intracerebral EEG generators (Dierks et al. 2000).

The version of LORETA that was implemented in the present study uses a three-shell spherical head model that includes scalp, skull, and brain compartments. EEG electrode coordinates were derived from cross-registrations between spherical and realistic head geometry (Towle et al. 1993). Both the head model and the electrode coordinates were coregistered to the Talairach brain atlas (Talairach and Tournoux 1988), digitized at the Brain Imaging Center of the Montreal Neurological Institute (MNI305; Collins et al. 1994). The source space (2,394 voxels at a voxel size of $7 \times 7 \times 7$ mm) was restricted to cortical gray matter and hippocampi as defined by the digitized MNI probability atlas. The LORETA functional images represent the electrical activity at each voxel as squared magnitude (i.e., power) of computed current density (unit: amperes per square meter, A/m²).

The recorded scalp electric potentials were used for computing the LORETA functional images. These functional images were computed for each subject separately, for the seven classical frequency bands (for technical details, see Frei et al. 2001).

The localization of the differences in activity between the two sessions in the seven frequency bands was assessed with voxel-by-voxel paired *t* tests of the log-transformed computed current density power. In addition, global, widespread differences (cluster analysis) were assessed by applying the exceedance proportion test (Friston et al. 1990). In all cases, the nonparametric randomization approach (Nichols and Holmes 2002) was used for estimating empirical probability distributions and the corresponding corrected (for multiple comparisons) critical probability thresholds.

Furthermore, for each of the seven frequency bands, Pearson's product-moment correlations between differences in current density (session t_1 –session t_0) and differences in the clinical severity measured with the MMSE (session t_1 –session t_0) were computed.

Results

Cognitive impairment

The cognitive impairment was assessed with the MMSE where scores range from 0 to 30, the optimum. All controls had an MMSE score of 30. The MMSE scores of the AD patients at t_0 (i.e., without rivastigmine medication) ranged between 10 and 27 (mean=19.1; SD=5.7), and was significantly lower compared to those of the controls ($p < 0.001$). At t_1 , the MMSE scores ranged between 10 and 29

(mean=19.2; SD=5.8): seven patients showed an improvement of their MMSE scores (mean score difference=+3.1 points; SD=2.41), and eight patients showed a worsening in their MMSE scores (mean score difference=−2.6 points; SD=2.07). One patient showed no difference between the two sessions. Across all patients, there was no difference of the MMSE scores between the two sessions. Table 1 shows the patient characteristics and MMSE scores at baseline and at the 3-months follow-up.

Spectral analysis

The comparison of the band power between the two groups at session t_0 , established the expected slowing of EEG frequencies in the AD patients: delta and theta increased significantly ($F(1,30)=6.73$, $p=0.015$; $F(1,30)=9.32$, $p=0.005$), and beta3 decreased significantly ($F(1,30)=5.53$, $p=0.026$) in AD patients compared to controls. Having confirmed the abnormal power spectrum of the AD patients, we focused on the rivastigmine effects in AD disease.

For AD patients, Fig. 1 exhibits the log-transformed mean power spectra across the 19 channels for sessions t_0 and t_1 (panel a), the mean values and 95% confidence interval for the difference between sessions (panel b), and their corresponding *p* values at each frequency bin (panel c). The power spectrum of the AD patients in session t_1 evidently shows lower values in the delta and theta frequency range. In the faster frequency range, the two distributions overlap, denoting similar values between the two sessions.

Comparing absolute band power between the two sessions, there was a significant decrease in delta ($F(1,15)=6.94$, $p=0.019$) and in theta ($F(1,15)=7.27$, $p=0.017$) in session t_1 compared to t_0 . No significant changes were observed for the other frequency bands. There were no significant interactions between session \times electrode location for delta or theta power. Figure 2 illustrates the significant differences of the follow-up *t* tests for the 19 channels: significant lower values in t_1 were observed for delta at ten channels and for theta at eight channels.

The computation of correlations between differences in frequency band power and differences in the MMSE scores between sessions t_0 and t_1 did not yield significant results. The smallest *p* value was reached in the delta frequency band ($r=-0.40$, $p=0.13$).

LORETA functional images of electric neuronal activity

The LORETA image statistics showed significant differences in cortical activity between the two sessions in two of the seven frequency bands, the two slow frequency bands of delta and theta. Figure 3 illustrates the brain areas where the AD patients had significantly weaker activity in session t_1 compared to session t_0 in these bands.

Table 1 Patient characteristics and MMSE scores at baseline and 3 months after the onset of rivastigmine medication

Subject	Gender (M/F)	Age (years)	MMSE Score	
			baseline	follow-up
1	M	64	19	17
2	M	70	15	17
3	F	72	14	13
4	M	74	22	25
5	M	75	25	29
6	F	75	15	16
7	F	77	20	14
8	F	77	15	23
9	F	77	10	10
10	M	78	26	21
11	F	78	25	24
12	F	80	24	20
13	M	82	11	10
14	M	84	27	26
15	F	85	24	25
16	M	90	14	17
Mean±SD		77.4±6.2	19.1±5.7	19.2±5.8

In the delta band, the cluster analysis resulted in the identification of three large clusters that reached $p=0.016$ (corrected). The largest cluster was localized at left-lateralized fronto-parietal regions. Voxel-by-voxel analysis in this cluster yielded $p<0.05$ (corrected) in Brodmann

Area (BA) 7 and BA 40 (superior parietal and inferior parietal, respectively). The second significant cluster grouped voxels at central parietal and cingulate regions, where the voxel-by-voxel analysis yielded $p<0.05$ (corrected) in BA 7 (precuneus). The third cluster included parahippocampal regions and the hippocampus bilaterally, where the voxel-by-voxel analysis yielded $p<0.05$ (corrected) in hippocampus and BA 36 (parahippocampal region).

In the theta band, a unique large cluster ($p=0.021$, corrected) at left-lateralized fronto-parietal regions was identified. Voxel-by-voxel analysis in this cluster yielded $p<0.03$ (corrected) in BAs 4, 7 and 40 (precentral, superior and inferior parietal lobule, respectively).

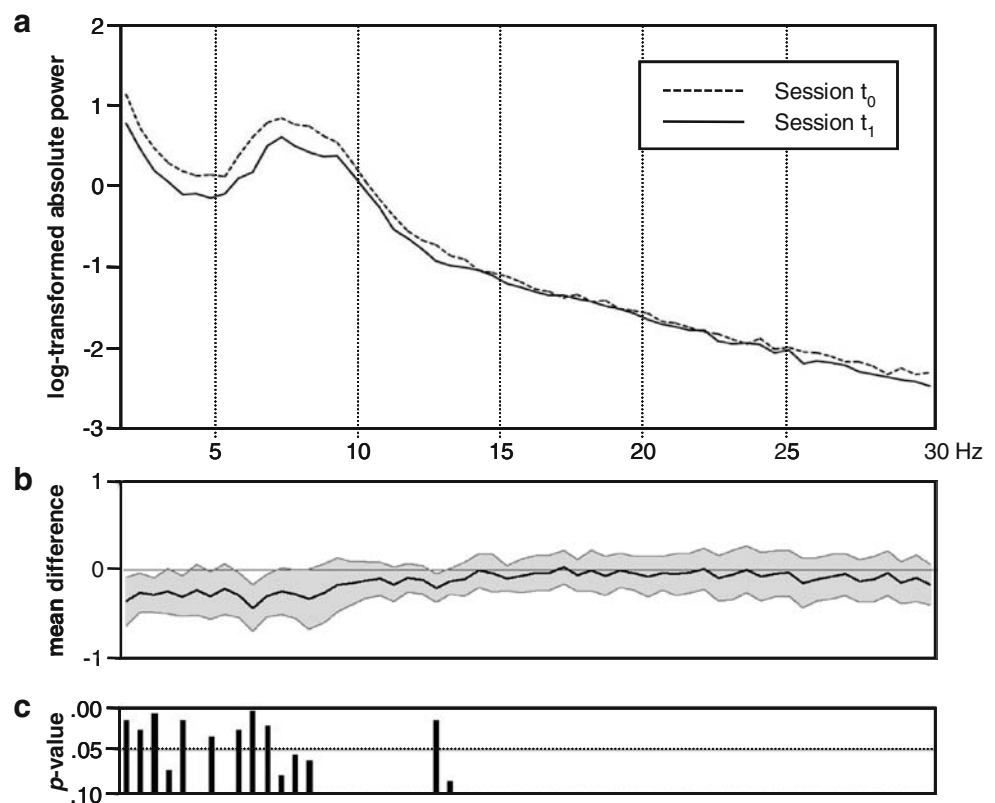
Table 2 gives a complete listing of all BAs that contained significantly different LORETA voxels.

Figure 4 displays the LORETA results in the alpha1 band that showed significant correlations between voxel current density and MMSE scores. The alpha1 band showed positive correlations in the left insula with a maximum in BA 13 ($r=0.57$, $p=0.02$), indicating better cognitive performance with increased alpha1 band power in this area.

Discussion

Four main findings have emerged from the present study. The first finding is that before rivastigmine treatment, the

Fig. 1 Power spectra before and 3 months after rivastigmine therapy. **a** The log-transformed mean absolute power spectra across the 19 channels of the two sessions; **b** mean values (black line) and 95% confidence interval (grey area) for the difference between sessions, and **c** their corresponding p values at each frequency bin



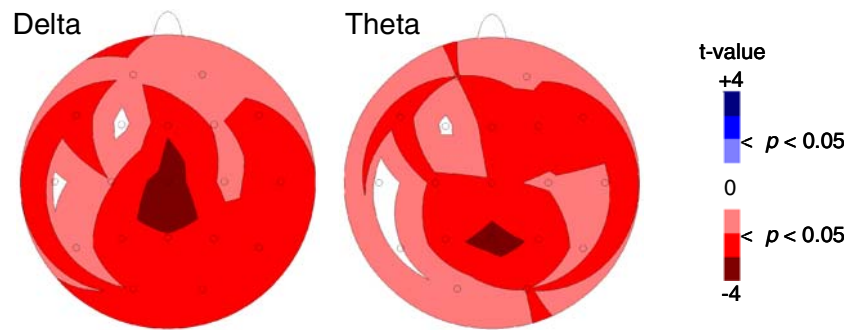


Fig. 2 T-maps illustrating the differences of EEG frequency band power between the two sessions t_0 and t_1 in delta and theta. Head seen from above, left ear left, nose up; the 19 electrode positions are

indicated by open symbols. t values are color-coded in steps of $t=1$ (see calibration scale). Decreased EEG power in session t_1 compared to t_0 in red

16 mild to moderate AD patients compared with their matched controls showed the expected slowing of their EEG frequency, i.e., increased power in slow frequency EEG activity (delta and theta frequency bands) and decreased power in fast frequency EEG activity (beta3 frequency band), in keeping with previous quantitative EEG results (e.g., Gianotti et al. 2007; Schreiter-Gasser et al. 1993), and thus validating the AD diagnosis of our patients from the electrophysiological perspective.

The other three findings concern the effects of 3 months of rivastigmine treatment in the AD patients, monitored with the MMSE that assessed global cognitive performance, and with the spontaneous EEG.

The global cognitive performance of the AD patients showed no significant differences between the two sessions, thus confirming the stabilizing effect of 3 months of rivastigmine on cognitive performances (e.g., Almkvist et al. 2004). In fact, the typical annual decline in untreated patients has been reported to be two to four points on the MMSE (Bullock and Dengiz 2005). Specifically, 8 of our 16 AD patients cognitively benefited from the treatment, in

line with previous observations that a positive response to the medication occurs on average in 30–70% of treated patients (e.g., Farlow et al. 2000; Feldman and Lane 2007).

Confirming our first hypothesis on spontaneous EEG, spectral analysis of the EEG data showed a significant power decrease in the delta and theta frequency bands during rivastigmine in our AD patients. These results agree with previous quantitative EEG studies that showed a shift of the power spectral EEG towards ‘normalization’. In particular, after short-term (5 days to 2 weeks) rivastigmine treatment, three previous studies showed a decrease of delta (Adler and Brassen 2001) and of theta (Adler and Brassen 2001; Adler et al. 2004; Brassen and Adler 2003). To our knowledge, the present paper is the first long-term (3 months) study that used rivastigmine and that reports a stabilization of these electrophysiological effects. Long-term studies conducted with other ChE-I (donepezil: Balkan et al. 2003; Kogan et al. 2001; tacrine: Jelic et al. 1998) also reported a ‘normalization’ of slow EEG frequency in AD patients.

Confirming our second hypothesis, LORETA localized long-term rivastigmine effects in a network that includes

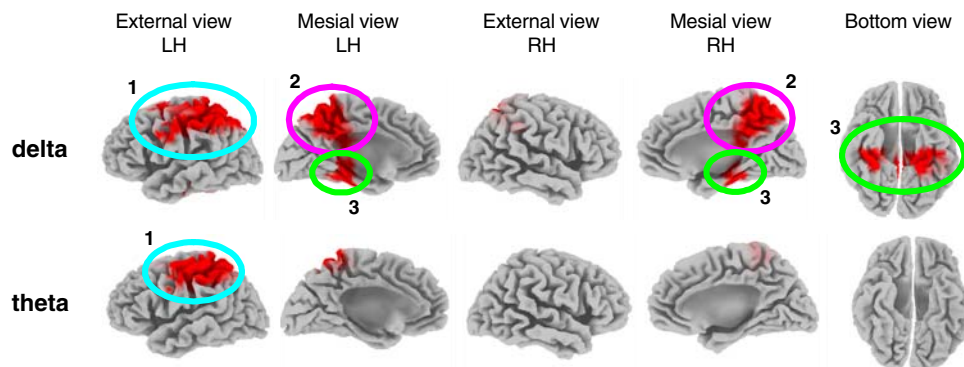


Fig. 3 LORETA-based statistical nonparametric maps (SnPM) illustrating the differences at $p < 0.05$ (corrected for multiple testing) of LORETA current density between the two sessions t_0 and t_1 in delta (upper part) and theta (lower part). Results are displayed on the ‘fiducial cortical surface’ (boundary midway through cortical thickness, Dickson et al. 2001). LH Left hemisphere, RH right hemisphere,

A anterior, P posterior, R right, L left. Cortex shown in gray scale; decreased activity in session t_1 compared to t_0 in red. Cluster no. 1: left fronto-parietal regions (light blue); cluster no. 2: central parietal and cingulate regions (pink), cluster no. 3: parahippocampal regions and the hippocampus (light green)

Table 2 Voxels of interest of the LORETA-based statistical nonparametric maps for assessing differences of activation between sessions t_0 and t_1 in AD patients in 2 EEG frequency bands

BA#	delta		theta	
	LH	RH	LH	RH
1	-	-	1	-
2	3	-	1	-
3	4	-	5	-
4	8	-	6	-
5	7	3	3	-
6	21	-	5	-
7	65	23	22	-
8	-	-	-	-
9	-	-	-	-
10	-	-	-	-
11	-	-	-	-
12	-	-	-	-
13	-	-	-	-
14	-	-	-	-
15	-	-	-	-
16	-	-	-	-
17	-	-	-	-
18	-	-	-	-
19	3	-	-	-
20	2	3	-	-
21	-	-	-	-
22	-	-	-	-
23	1	1	-	-
24	-	-	-	-
25	-	-	-	-
26	-	-	-	-
27	1	1	-	-
28	-	-	-	-
29	1	1	-	-
30	3	-	-	-
31	11	10	-	-
32	-	-	-	-
33	-	-	-	-
34	-	-	-	-
35	4	3	-	-
36	9	9	-	-
37	4	2	-	-
38	-	-	-	-
39	1	-	-	-
40	42	-	32	-
41	-	-	-	-
42	-	-	-	-
43	-	-	-	-
44	-	-	-	-
45	-	-	-	-
46	-	-	-	-
47	-	-	-	-
hipp.	6	5	-	-
TOTAL	196	61	75	0

The number of voxels sorted by Brodmann areas (BA number, first column) are listed separately for the *left* (LH) and for the *right* hemisphere (RH). Colors mark the different clusters, and refer to Fig. 3.

three spatial clusters in frontal, parietal, and temporal regions. Specifically, during medication, left fronto-parietal regions showed a significant decrease of delta and theta frequency activity. Moreover, delta activity significantly decreased in the posterior cingulate cortex, and bilateral in parahippocampal regions and in hippocampus. We note that a decrease of delta and theta activity corresponds to an increase of cortical activation in the concerned regions (Buchan et al. 1997).

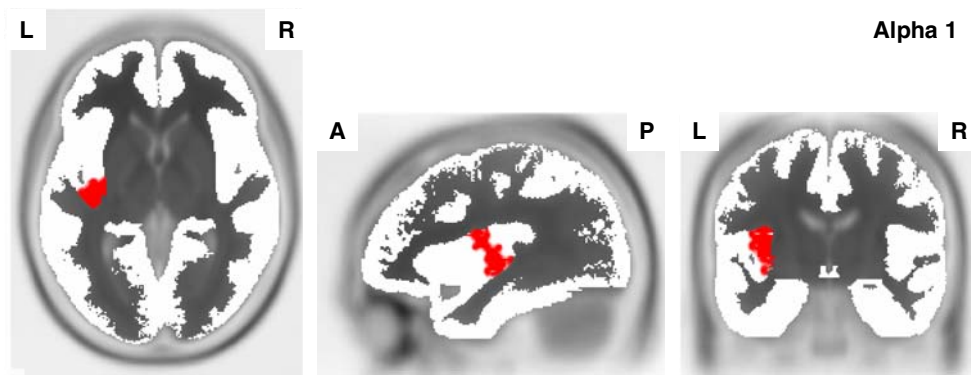
AD patients compared to healthy controls consistently showed decreased activity in medial temporal lobe structures such as parahippocampal regions and in the hippocampus as shown in fMRI studies (e.g., Celone et al. 2006; Machulda et al. 2003; Small et al. 1999) and in SPECT and PET studies (e.g., Bradley et al. 2002; see Matsuda 2001, for a review). Medial temporal lobe structures and the hippocampus are among the first regions targeted by AD pathology (Braak and Braak 1991) and are key regions for memory functions, especially episodic memory, whose impairment is the hallmark of early AD (Hyman et al. 1984). Reduced metabolism in the posterior cingulate cortex and precuneus are also a common finding in early AD (Bradley et al. 2002; Matsuda 2001; Minoshima et al. 1997).

The present results demonstrate an increase of cortical activity due to rivastigmine medication in regions that are well known to be affected in AD already at an early stage of the disease. In line with our EEG-based results, a series of PET and SPECT studies demonstrated hypermetabolism or hyperperfusion after ChE-I medication in AD patients in fronto-parietal regions (Bohnen et al. 2005; Ceravolo et al. 2004; Mega et al. 2001; Stefanova et al. 2006), in posterior cingulate (Bohnen et al. 2005; Ceravolo et al. 2004), and in parahippocampal or hippocampal regions (Mega et al. 2001).

The cortical regions that were affected by rivastigmine medication in the present study overlap with the recently proposed *hippocampal-parietal memory network* (Vincent et al. 2006). Vincent et al. (2006) were concerned with the hypothesis that parietal cortex contains areas associated with the medial temporal lobe memory system. In their fMRI study, they examined correlations in spontaneous BOLD fluctuations in different brain areas. This novel approach focused on the surprising observation that spontaneous activity at resting state (i.e., in the absence of overt task performance) consistently and repeatedly exhibits a coactivation in a distributed network of cortical regions, the so-called default-mode networks (e.g., Gusnard and Raichle 2001; Raichle et al. 2001).

The topographic convergence of our results with the memory network proposed by Vincent et al. (2006) leads to the speculation that rivastigmine in our AD patients specifically activates brain regions that are involved in

Fig. 4 Axial, sagittal, and vertical slices centered at the voxel of strongest correlation ($X=-38$, $Y=-11$, $Z=1$ in Talairach coordinates) showing in red results of voxelwise Pearson's product-moment correlation ($p < 0.05$) between difference in current density (session t_1-t_0) in the alpha 1 band and difference in MMSE scores (session t_1-t_0)



memory functions, notably a key symptom in this degenerative disease.

To our knowledge, this is the second EEG LORETA-based study focusing on ChE-I effects in AD. The other study (Babiloni et al. 2006b) did not show any shift towards normalization in the cortical activity after 1 year of donepezil. Contrary, they reported a significant increase in the slow delta and theta frequencies and a significant decrease in the alpha band after treatment. These observations actually indicate a progressive cortical degeneration during the study year despite of the treatment. The reason of the discrepant results between the two EEG LORETA studies is probably in part to refer to the different durations of the studies: AD is a progressive disease and even if ChE-I treatment has been reported to be useful in psychological and in physiological measurements, it is to be assumed that the degeneration of cortical projection of cholinergic neurons will progress, and therefore, after a certain time, the initial benefits of the treatment will vanish. Nevertheless, Babiloni et al. (2006b) reported a less dramatic decrease of activity in the alpha1 band in occipital and temporal regions in the group of AD patients that were recognized as ‘responders’ (based on the MMSE scores) compared to the ‘nonresponders’. This result is particularly interesting and very in line with the correlation results reported in the present study. Our data showed a significant correlation in the alpha1 band between the differences in the cognitive functions measured with MMSE during the two sessions and LORETA-computed intracortical activity in the left insula, indicating better cognitive performance with increased alpha1 current density.

A previous study by our group found that in a group of non-medicated mild to moderate AD, increased alpha1 activity in left temporal cortical areas was associated with better cognitive performances (Gianotti et al. 2007). It is worthy to note that, the insula is strongly reciprocally interconnected with temporal regions (Shelley and Trimble 2004). A volumetric MRI study showed that mild to moderate AD patients have significantly more atrophy of the insula (together with the hippocampus and the parietal

cortex) than healthy age-matched controls (Foundas et al. 1997). PET studies in healthy subjects have found that the activation of the insula was associated with verbal memory tasks (Grasby et al. 1994; Paulesu et al. 1993). Of particular interest for the present results, verbal memory impairment was shown after left but not right insular cortex infarction (Manes et al. 1999). It appears that the left insula is part of a functional neuroanatomical circuit that is involved in verbal (semantic) memory and that is impaired in AD. Based on the present results, we speculated that AD patients that cognitively benefited from medication—possibly via a reduction of verbal memory impairment—showed an increase of alpha1 EEG activity in the left insula.

In light of the present EEG results, the lack of a statistical significant global cognitive amelioration measured with the MMSE, might appear surprising at first sight. There are some indications that treatment with ChE-I not only stabilizes cognitive function in a *global* sense, but also has positive effects on *specific* cognitive functions such as attention rather than episodic memory (tacrine medication, Almkvist et al. 2001). As said above, we speculated based on the present neuroimaging results that rivastigmine possibly reduces the verbal memory impairment of mild to moderate AD patients. Future studies that combine neurophysiological measurements with cognitive/neuropsychiatric measurements should use a more detailed cognitive assessment. The latter should unfold the MMSE single measure into contributing subfactors so that the specific cognitive effects of treatment become available. Such widened cognitive assessment would offer an array of testable correlations between the spectrum of cognitive measurements and the spectrum of neurophysiological measurements, thereby possibly enhancing the agreement between measurements.

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